OReX: Object Reconstruction from Planner Cross-sections Using Neural Fields

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Abstract

Reconstructing 3D shapes from planar cross-sections is a challenge inspired by downstream applications like medical imaging and geographic informatics. The input is an in/out indicator function fully defined on a sparse collection of planes in space, and the output is an interpolation of the indicator function to the entire volume. Previous works addressing this sparse and ill-posed problem either produce low quality results, or rely on additional priors such as target topology, appearance information, or input normal directions. In this paper, we present OReX, a method for 3D shape reconstruction from slices alone, featuring a Neural Field as the interpolation prior. A simple neural network is trained on the input planes to receive a 3D coordinate and return an inside/outside estimate for the query point. This prior is powerful in inducing smoothness and self-similarities. The main challenge for this approach is high-frequency details, as the neural prior is overly smoothing. To alleviate this, we offer an iterative estimation architecture and a hierarchical input sampling scheme that encourage coarse-to-fine training, allowing focusing on high frequencies at later stages. In addition, we identify and analyze a common ripple-like effect stemming from the mesh extraction step. We mitigate it by regularizing the spatial gradients of the indicator function around input in/out boundaries, cutting the problem at the root. Through extensive qualitative and quantitative experimentation, we demonstrate our method is robust, accurate, and scales well with the size of the input. We report state-ofthe-art results compared to previous approaches and recent potential solutions, and demonstrate the benefit of our individual contributions through analysis and ablation studies.

1. Introduction

Reconstructing a 3D object from its cross-sections is a long standing task. It persists in fields including medical imaging, topography mapping, and manufacturing. The typical setting is where a sparse set of arbitrary planes is given, upon which the 'inside' and 'outside' regions of the depicted domain are labeled, and the entire shape in 3D is to be estimated (see Fig. 1). This is a challenging and illposed problem, especially due to the sparse and irregular nature of the data. Classical approaches first localize the problem by constructing an arrangement of the input planes, and then introduce a local regularizer that governs the interpolation of the input to within each cell. While sound, these approaches typically involve simplistic regularization functions, that also only interpolate the volume within a cell bounded by the relevant cross-sections; as a consequence, they introduce oversmoothed solutions that do not respect features. In addition, finding a cellular arrangement of planes is a computationally-heavy procedure, adding considerable complexity to the problem, rendering it quickly infeasible for large inputs (see Section 4). Note that, as we demonstrate (Section 4), recent approaches reconstructing a mesh from an input point-cloud are not well suited to our setting, as they assume rather dense sampling of the entire shape. In addition, these methods do not consider the information of an entire cross-sectional plane, but rather only on the shape boundary.

In this paper, we introduce *OReX*—a reconstruction approach based on neural networks to estimate an entire shape from its cross-sectional slices. Similar to recent approaches, the neural network constitutes the prior that extrapolates the input to the entire volume. Neural networks in general have already been shown to inherently induce smoothness [17], and self-similarities [12], allowing natural recurrence of

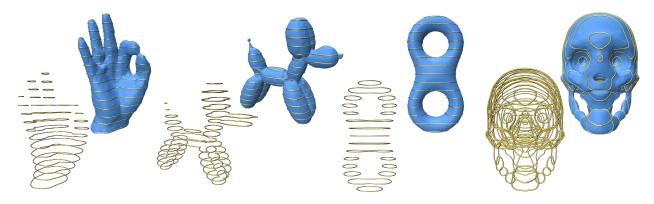


Figure 1. OReX reconstructs smooth 3D shapes (right) from input planar cross-sections (left). Our neural field-based prior allows smooth interpolation between slices while respecting high-frequency features and self-similarities.

patterns. Specifically, we argue that Neural Fields are a promising choice for the task at hand. Neural Fields represent a 3D scene by estimating its density and other local geometric properties for every given 3D coordinate. They are typically trained on 2D planar images, and are required to complete the entire 3D scene according to multi-view renderings or photographs. This neural representation is differentiable by construction, and hence allows native geometric optimization of the scene, realized via training. We pose the reconstruction problem as a classification of space into "in" and "out" regions, which are known for the entire slice planes, and thus generate the indicator function which its decision boundary is the output shape.

The main challenge with applying Neural Fields to this problem is high frequency details. Directly applying established training schemes [19] shows strong spectral bias, yielding overly smoothed results and other artifacts (Fig. 9). Spectral Bias is a well known effect, indicating that higher frequency is effectively learned slower [22]. To facilitate effective high-frequency learning, avoiding the shadow cast by the low frequency, we introduce two alterations. First, we sample the planar data mostly around the inside/outside transition regions, where the frequencies are higher. This sampling is further ordered from low to high frequency regions (according to the distance from the inside/outside boundary), to encourage a low-to-high frequency training progression. In addition, we follow recent literature and allow the network to iteratively infer the result, where later iterations are responsible for finer, higher-frequency corrections [1, 23].

Finally, we consider another high frequency artifact, also found in other neural-field-based works [9]. The desired density (or indicator) function dictates a sharp drop in value at the shape boundary. This is contradictory to the induced neural prior, causing sampling related artifacts in the downstream task of mesh extraction (Sec. 3.4). To alleviate this, we penalize strong spatial gradients around the in/out boundary contours. This enforces smoother transition between the in and out regions, allowing higher quality mesh extraction.

As we demonstrate (see Figure 1), our method yields state-of-the-art reconstructions from planar data, both for man-made and organic shapes. The careful loss and training schemes are validated and analyzed in quantitative and qualitative experimentation. Our method is arrangement-free, and thus both interpolates all data globally, avoiding local artifacts, and scales well to a large number of slices (see Section 4). Code and data will be made available.

2. Related work

Reconstruction from cross-sections Reconstruction from planar cross-section has been a long-standing challenge in geometry processing and computational geometry. The problem was mostly studied in the parallel planes setting (e.g., [2, 3, 5]), where the 3D object was reconstructed per two such "keyframes". Later work offered general solutions for any orientation or distribution of planes [4, 16]. The general approach was based on tessellating the planes into convex cells by the planes of the arrangement, and reconstructing the object in each cell, by defining some interpolant inside it. These methods suffer from several issues: the construction of the arrangement is computationally expensive (with at least cubic asymptotic times), and the local reconstruction introduce continuity artifacts (see Section 4). Furthermore, the interpolants were usually designed for smoothness or proximity, and fail to capture more global trends in the geometry of the slices, such as twists or extrusions (see Figure 6). Some works provide topological guarantees [14, 26] or limited the solution to given templates [13], but do not provide a general solution without these priors. Our work is arrangement-free and provide a flexible high-parameteric model, using neural networks, to capture the details of the reconstructed object.

Neural reconstruction Most recent reconstruction work employing neural networks address reconstruction from

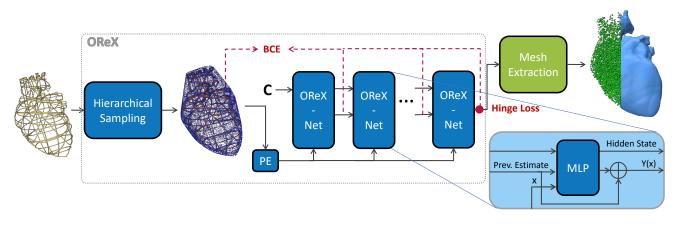


Figure 2. OReX method overview. The input (left) is a set of planar cross-sections with inside/outside information on them. The planes are sampled into points in a hierarchical scheme, which are fed to our iterative Neural Field for training. After training, the final shape is estimated using an off-the-shelf mesh extractor.

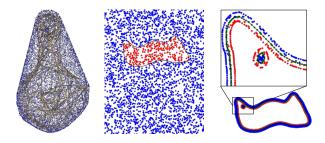


Figure 3. We train OReX on three types of sampling distributions of the input: A scaled up version of the 3D convex hull bounds the reconstruction volume (left); Uniform sampling within each plane helps stabilize the learning (middle); Most of the samples are concentrated where accuracy matters most - on and around the boundary contours on the input planes (right).

dense point clouds. Our problem could be cast as a point cloud reconstruction one, after sampling the planes. Indeed in this regime the high frequency problem is pronounced as in our case, and even more so since more information regarding the target shape is available. Almost all recent approaches employ an implicit representation of the shape. Some works populate 3D (sometimes adaptive) grids to handle fine-details [7, 8, 18, 24], which is challenging to scale, or perform local operations [6, 21], which rely on a rather dense neighborhood. To alleviate this, a mesh can be directly optimized to match the input [12]. Other neural fields have been employed as well in this context [17], without additional information such as normals. See a recent survey for more approaches [25]. As we demonstrate (Section 4), this general line of works employ weaker priors, which do not fit the sparse nature of our problem well.

Perhaps a more similar setting is the one of reconstruction from projections or photographs. Here the reconstructions are from 2D data as well, which is also of sparser nature, albeit using appearance information which we do not. Literature in this field is deep and wide, with several surveys [10,11], including the usage of neural fields. In spite of this work, we start from a basic neural field baseline. We argue our work is orthogonal to that listed here, as it can be plugged in to replace our baseline. We leave for future work to inspect the most performing architecture. Addressing the most similar problem setting, concurrent work by Ostonov et al. [20] employ reinforcement learning and orthographic projections to ensure proper reconstruction. Except for requiring additional information during inference, they also require a training phase, and are restricted to the domain trained on. Our approach, in contrast, requires no additional information besides the planes, neither for the test-time example, nor a large dataset.

3. Method

We next lay out the details for effective high-quality shape reconstruction from slices. Our approach is based on a neural field, *OReXNet*. OReXNet outputs Y(x), an extrapolation of the inside/outside indicator function for a query point $x \in \mathbb{R}^3$ (Sec. 3.1). Given a single set of input cross-sections, the network undergoes training to approximate the target function on the input. After training is complete, Y is sampled on the entire volume, and a resulting shape is extracted using the Dual Contouring (DC) approach [15]. This pipeline is depicted in Fig. 2.

As motioned in Sec. 1, the main challenge in reconstruction quality is high-frequency details. The straightforward approach to our problem would be to train a Neural Field for the desired indicator function by uniformly sampling all planes, and subsequently train a network using a *Binary Cross Entropy* (BCE) loss on all sampled points. Typical approaches also represent the input coordinates using Positional Encoding (PE) [19]. As it turns out, this approach yields overly smooth results failing even to interpolate the input (Fig. 9). To improve reconstruction fidelity, and allow higher frequency details in the resulting shape, we introduce two alterations to the aforementioned training scheme. We present our hierarchical input sampling scheme in Sec. 3.2, and our iterative-refinement architecture in Sec. 3.3.

Finally, we also address a common artifact in implicit mesh extraction [9]. Repeating patterns can be seen that correlate to the sampling pattern of the mesh extraction phase, as demonstrated in Fig. 8. We describe how we design the loss function to mitigate this artifact in Sec. 3.4. See the Supplementary material and code for implementation details and hyper-parameter values.

3.1. Problem Setting

We consider a set $\mathcal{P} = \{P_1, \dots, P_k\}$ of 2D planes embedded in \mathbb{R}^3 , with arbitrary offset and orientation. Each plane P_i contains an arbitrary set of (softly) non-intersecting oriented contours $C_i = \{c_{i,1}, \dots, c_{i,l_i}\}$ that consistently partition the plane into regions of "inside" and "outside" of an unknown domain $\Omega \subset \mathbb{R}^3$ with boundary $\partial\Omega$ (Fig. 2). The target output of our method is an indicator function $Y : \mathbb{R}^3 \to \mathbb{R}$, defining Ω as:

$$Y(x) = \begin{cases} 1 & x \notin \Omega \\ 0 & x \in \Omega \\ 0.5 & x \in \partial \Omega \end{cases}$$
(1)

In practice, we approximate Y using a function f, such that $Y(x) \approx \sigma(f(x))$, where $\sigma(z) = \frac{1}{1+e^{-z}}$ is the sigmoid function.

3.2. Input Sampling

Regularly or randomly sampling the input planes for training yields inaccurate and overly smooth results (see Figure 9). Instead, we define three types of relevant point distributions to sample from, as depicted in Figure 3:

- 1. We bound the reconstructed volume by the 3D convex hull of all the input contours, and scale it up by 5%. We then sample it uniformly, and all the sampled points get "outside" labels.
- 2. We compute the bounding box (aligned to the principal axes) of the contours in each plane, and sample it with uniform distribution.
- 3. Importantly, most samples should be taken from the boundary's vicinity, as this is the region where accuracy matters most. To do this we sample every contour edge evenly, and further sample for each of these points off-surface points of varying distance. Off-surface locations are found by moving away from the contour on

the plane (i.e., by adding the direction that is both orthogonal to the plane normal, and the contour tangent). Similarly, we sample on-plane off-surface points in a circle around each vertex.

Each sampling point x_i is matched with a label Y_i according to the information on the slice, and the pairs $\{x_i, Y_i\}$ constitute the input to our training. See supplementary material for hyperparameters definition and values.

Frequency-Oriented Sampling. In order to encourage better high-frequency learning, we sample the 3^{rd} type of points around a set of varying distances, from 0.1% of the total size away from the contours to three orders of magnitude closer. In every epoch, we only use points sampled around three consecutive distance ranges. For early training iterations, we use the three largest distances, since further away points translate to lower frequency information about the shape. As the training progresses, and the lower frequencies are assumed to stabilize, we expose to the network to points that grow closer and closer to the actual contour, thus focusing the learning process on higher and higher frequencies (see Figure 11). See the Supplementary Material for more details and exact scheduling.

3.3. Architecture

OReXNet is simply an MLP that takes a 3D coordinate as input, represented using positional encoding, and produces the function Y (Section 3.1) at any query point. In order to encourage high frequency details, we introduce an iterative refinement mechanism. Inspired by recent work, we allow the network to refine its own results by running them through the network for a small number of iterations. This process was previously shown to produce a coarse-to-fine evolution in the realm of 2D images [1], and we argue it applies to our case as well. As demonstrated in Fig. 2, ORexNet is hence a *residual* MLP that is fed the result of the previous iteration, and a small hidden state code, along with the query point. These iterations (10 in our experiments) are performed both during training and inference, where at inference time only the last result is taken, and during training the loss is applied to the results of all steps. The first iteration starts from a learned constant C. We show that this process indeed sharpens features and allows the incorporation of higherfrequency details in Figure 12.

3.4. Loss Function and Inference

In order to present our loss function, we must first attend to an issue in the final stage of our pipeline. In this stage, we extract an explicit mesh for the boundary of the indicator function using Dual Contouring [15]. This step uses a discretely sampled version of Y(x) and $\nabla Y(x)$ on a regular 3D grid to extract the mesh. As can be seen in Fig. 8 (and as witnessed other works [9]), this creates a ripples-like artifact, that correlates to the 3D grid resolution. This results

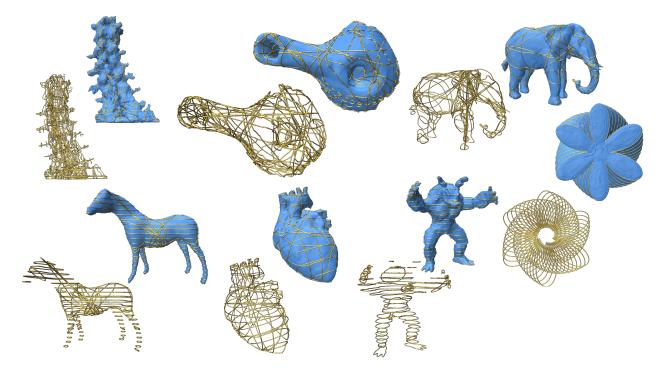


Figure 4. Results parade. A qualitative demonstration on a collection of man-made and medical inputs. Zoomed-in viewing recommended.

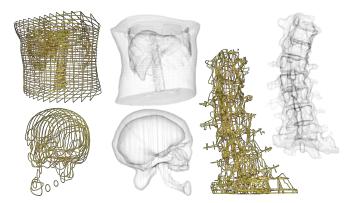


Figure 5. Additional qualitative results, where an internal view depicts reconstructions of internal cavities and tunnels. Zoomed-in viewing recommeded.

from an aliasing of the sampling in these regions where the gradient magnitudes exhibit high variance. This effect could be mitigated via higher resolution grid sampling, which is expensive, or a post-process operation that may compromise the geometry. Instead, we propose revisiting the loss function of the training process, and incorporating regularization to reduce this sharp drop in value at the shape boundary. First, we omit the activation—in other words, we use the function f(x) for contouring, while using Y(x) only for training (Sec 3.1). This de-radicalizes the function values, already offering a softer transition between inside and outside

regions. In addition, we explicitly penalize strong transitions by using a *hinge loss* (Eq. 2). With this, we reduce the gradient magnitude variance considerably by limiting them close to the input shape boundary. Our loss function hence for a single query point is:

$$\mathcal{L}(x,\theta) = \sum_{i=0}^{N-1} \text{BCE}(Y_i(x)) + \lambda \max\left(0, ||\nabla f_{N-1}(x)|| - \alpha\right)$$
(2)

Where σ is the sigmoid function, θ are the parameters of the network, BCE() is the binary cross-entropy loss applied to all outputs of our iterative scheme, max(0, x) is a hinge loss applied only to the last iteration, N the number of iterations, and α and λ are hyperparameters. Fig. 8 demonstrates the correction effect of the hinge loss.

4. Experiments

To evaluate our method, we have developed a prototype, and ran it on a rather weak NVIDIA GeForce GTX 1080 Ti. Please see the Supplementary Material for exact timing and memory consumption statistics, but generally speaking all training processes took less than four hours on the single GPU.

4.1. Results and Comparisons

We first qualitatively demonstrate the result of our method on a variety of slice inputs, from both the medical and graphics worlds (Fig. 4). This demonstrates the versatility and generality of our method. We further show our our algorithm correctly reproduces the internal cavities and details of reconstructed objects in Fig. 5. Note how sharp details are learned along side a smooth interpolation between slices, leaving no slice transition markings on the resulting shape.

In terms of other methods, we qualitatively (Fig. 6) and quantitatively (Table 1) compare our method to Bermano et al. [4], which is a reconstruction from cross-section method with the same input-output as ours. We further compare to general state-of-the-art reconstruction methods that target point clouds [12]. Hanocka et al. [12] expect point normals as input as well. Hence we compare our result to the latter work with Ground Truth (GT) normals at input, and with ones coming from the input plane normals for a more correct comparison. Quantitatively, we use the following metrics: 1) intersection-over-union of inside regions in reconstructed volumes and 2) GT planes, and 3) symmetric hausdorff distance. These metrics demonstrate our superiority over the compared methods. See Supplementary Material for more comparisons.

Scalability We show our method does not suffer the computational cost that arrangement-based methods [4, 14, 16] must bear, since we do not tessellate the space, and hence scale well with the input. In addition, we show (Fig. 7) how our method converges with the addition of slices.

4.2. Ablations

We perform ablation testing to evaluate important aspects of our method and our design choices.

Gradient magnitude regularization (Fig. 8) We show the effect of the hinge-loss regularizer on gradient magnitudes, with increasing λ values. It is evident the hinge loss effectively filters out the high variance, and smooths the ripple artifacts.

Choice of architecture and sampling (Fig 9) We justify our design choices by training a baseline architecture with uniform grid sampling and no iteration refinement. It is evident such a model does preserve details nor interpolate well, even for a relatively simple case.

5. Conclusions

We have presented OReX, a state-of-the-art method for long standing problem of shape reconstruction from nothing but planar in/out cross-sectional indicator data. Being free of dataset and training requirements, OReX is simple and intuitive to use. Our work balances the smoothness of a neural prior with high-frequency features, through three insights into the training process and architecture. We show our approach successfully produces smooth interpolation between contours while respecting high frequency features and repeating patterns. In addition, we believe some of the analysis and insights presented here can be applied to neural fields for other tasks as well.

Of course, the advantage of the method is also its disadvantage. Using only binary data, much of the information is lost in the process. For example, for medical imaging an interesting future direction would be to inspect using the raw continuous results of a planar probe such as an Ultra-Sound one. This will provide the system with more information compared to the in/out segmented version of it used at the moment. Another interesting avenue for research is extending this work for multi-labeled volumes (e.g., the reconstruction of several organs simultaneously from a scan), and using partial or noisy data. We hope this work would be us a step closer to an easy to use, computationally friendly, production grade reconstruction capabilities.

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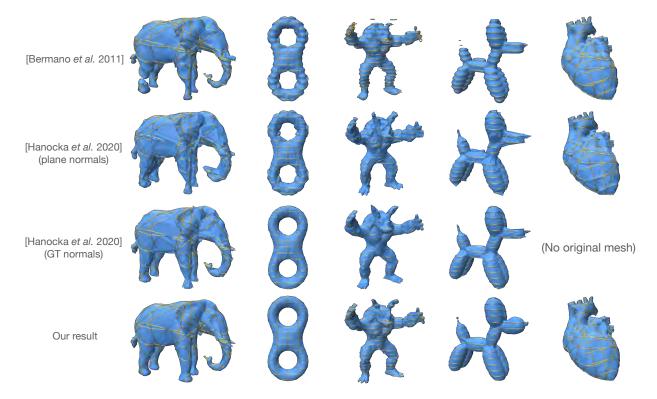


Figure 6. Qualitative comparisons to other approaches. Our result is smoother, more aligned to features, and with less artifacts. Note how the reconstructed shape silhouettes does not suffer imprints from the input planes. Check Table 1 for quantitative comparison.

		Hausdorff distance		IoU in 3d					IoU in 2d			
Input	OReX	Bermano et. al	point2mesh	point2mesh	OReX	Bermano et. al	point2mesh	point2mesh	OReX	Bermano et. al	point2mesh	point2mesh
			plane normals	GT normals			plane normals	GT normals			plane normals	GT normals
Eight 15	0.018	0.065	0.219	0.046	0.984	0.865	0.842	0.961	0.988	0.984	0.795	0.980
Eight 20	0.006	0.033	0.045	0.014	0.987	0.893	0.915	0.974	0.986	0.976	0.961	0.971
Elephant	0.056	0.081	0.100	0.086	0.966	0.908	0.885	0.935	0.975	0.969	0.850	0.908
Balloon dog	0.049	0.194	0.078	0.086	0.957	0.868	0.897	0.928	0.988	0.977	0.926	0.956
Hand OK	0.063	0.177	0.195	0.135	0.955	0.860	0.921	0.931	0.987	0.968	0.908	0.882
Armadillo	0.050	0.121	0.057	0.059	0.939	0.891	0.891	0.921	0.964	0.776	0.850	0.868

Table 1. Quantitative comparisons. We measure performance using Hausdorff distance, IoU of the inner volume compared to the GT shape, and IoU of the inner surface on the input cross-sections. We compare our result to a dedicated cross-section based reconstruction method [4], and to two flavors of a pointcloud reconstruction method [12]. See more comparisons in the Supplementary Material.

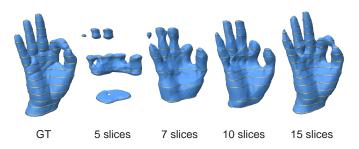


Figure 7. Qualitative evaluation on quality evolution with the amount of given slices. As can be expected, introducing more slices converges consistently converges to a closer solution.

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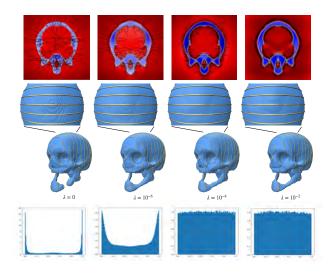


Figure 8. Illustration of our Hinge loss effect for mitigating ripplelike aliasing artifacts. Output values of our network sampled on an input plane. Red - outside, blue - inside, black arrows - value gradient. Middle: The reconstruction mesh for different regularization intensities, with a closer view on the top of the skull. As can be seen, regularization intensity effectively reduces gradients at shape boundaries, restraining the aliasing artifacts. Bottom: distribution of vertices along grid edge during mesh extraction. The hinge regularization clearly brings more flexibility by allowing placing vertices also in the middle of the sampled grid cells, and not only on their edges. Zoomed-in viewing recommended.

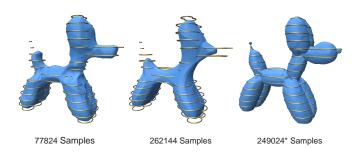


Figure 9. Left and middle: the baseline experiment with regular grid samples of 64 and 128 resolution over the slices. Right: our result for the same amount for samples (our variable number of samples is provided at its mean).

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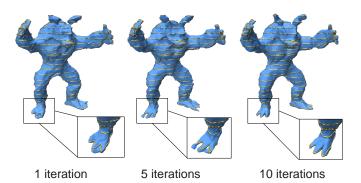


Figure 10. Iterative refinement experiment. Training and infering with more OReXNet refinement iterations allows the network to perform smaller scale corrections and reduces spectral bias.

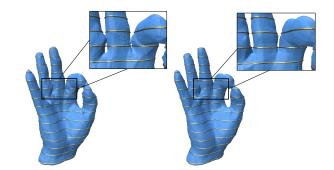


Figure 11. Left: non-hierarchical sampling, i.e., using points from all off-surface distances uniformly. Right: results using our hierarchical sampling scheme.

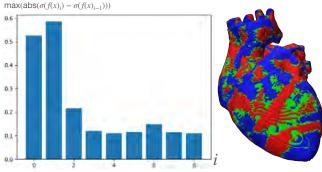


Figure 12. Refinement progression throughout the iteration process. The maximum change in the output value decreases along the iterations. Right: points that were added to the shape (Red) and that were removed from it (blue) in the last refinement iteration. These are concentrated on the level set, whereas most other points (green, covering all internal regions) have already converged.

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